A Tale of Two Legs: Maintaining Dynamic Stability in A-P and M-L Directions in Persons with Unilateral Transtibial Limb Loss

Georgia | College of Tech | Sciences School of Applied Physiology

Darren Bolger, B.S. Andrew Sawers, Ph.D. Lena Ting, Ph.D.

Neuromechanics Laboratory Georgia Institute of Technology Atlanta, GA, USA



Introduction

- Falling remains a significant concern among individuals with lower limb loss, with over 50% of those surveyed having fallen in the past year [1].
- Although lateral instability has been shown to predict fall risk in the elderly [2], little is known about medial-lateral (M-L) dynamic balance in persons with transtibial limb loss (TTLL).
- Previous work has focused on static balance and dynamic balance in anterior-posterior (A-P) directions.
- Platform perturbations are useful to understand postural strategies under dynamic conditions [3] and may be used to predict balance capabilities [4].
- The **objective** of this study was to characterize dynamic balance control of individuals with TTLL across multiple directions.
- We **hypothesized** that individuals with TTLL would have a **smaller** stability margin as compared to unimpaired participants.

Methods

We examined responses to multi-directional perturbations at a standardized stance width.

- Four males with unilateral TTLL (AMP) and four age and gender matched unimpaired adults (CONT) participated.
- Ramp and hold perturbations in twelve evenly-distributed (0-330°) directions were randomly applied.
- Stance width was equal to subject inter-ASIS distance [5].

We calculated peak COM and COP displacements during a defined period. Center of Mass (COM):

COM calculated using subject anthropometrics and Vicon markers.

Center of Pressure (COP):

Individual foot and cumulative COP calculated from ground reaction forces and moments recorded by force plates under each foot.

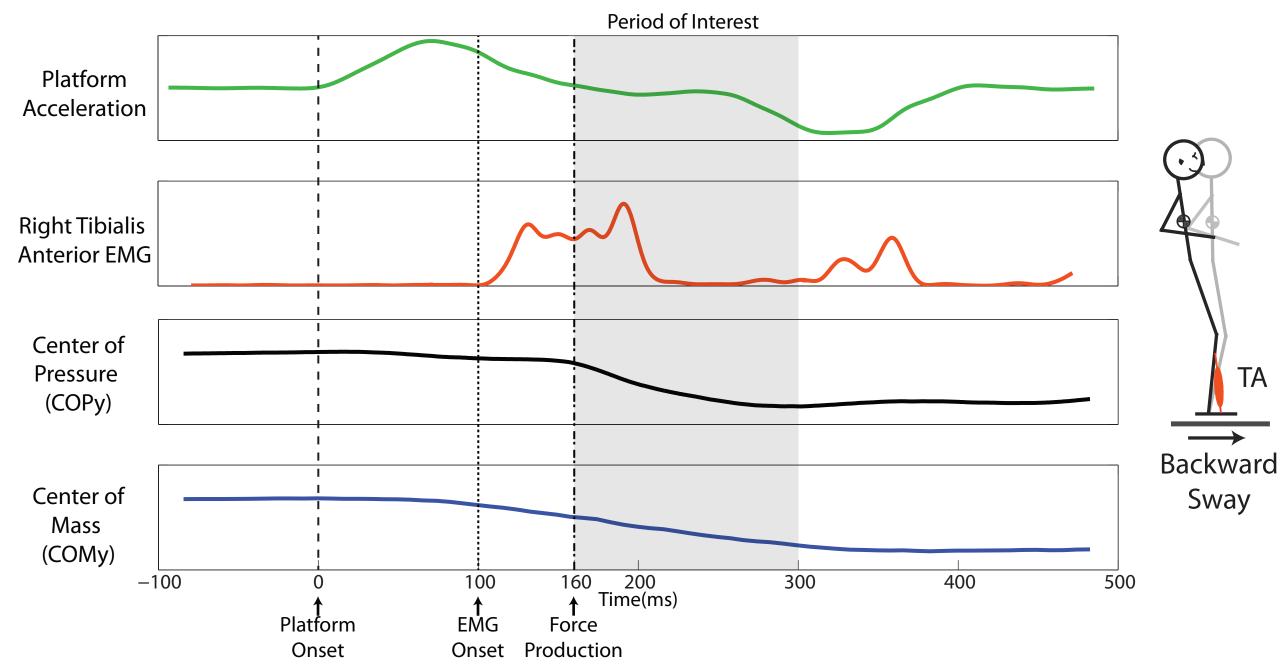
Stability Margin:

- Stability margin = peak COP peak COM
- Smaller stability margin represents increased likelihood of losing balance [6].

Data Analysis:

- Peak COM and COP determined from time period of 160-300 ms after platform onset (see figure below).
 - Begins after force production onset (160 ms) and ends prior to peak platform deceleration (300 ms) to limit effect of platform kinematics.
- Two-way mixed-design ANOVAs were performed for each dependent variable ($\alpha = 0.05$).

Representative Control Subject - 90° Perturbation (Backward Sway)



Acknowledgments

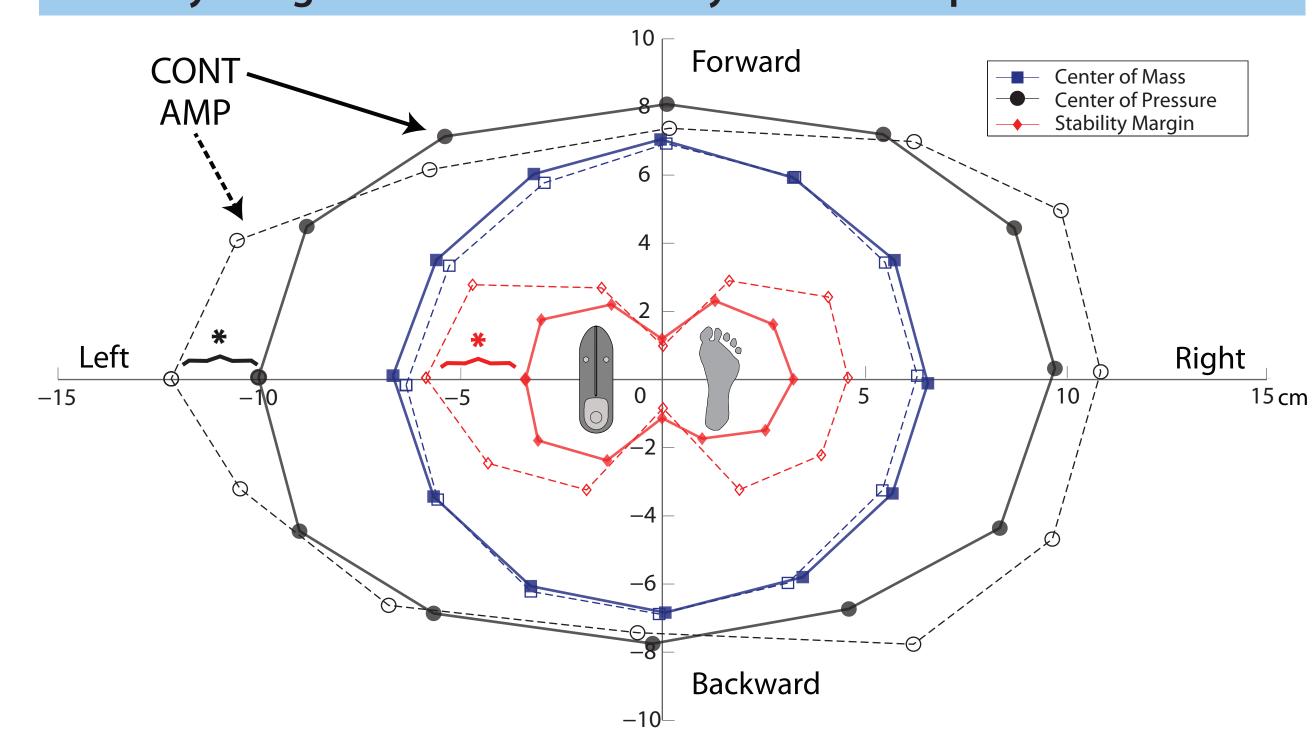
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Results

Stability margin increased with sway toward the prosthetic limb.



- **Stability margin** was significantly greater (*p=0.012) in AMP group during lateral sway toward the prosthetic limb.
- This increase was due to a larger COP displacement (*p=0.012) rather than a reduction in **COM displacement**.
- Stability margin did not differ between groups for any of the other cardinal directions analyzed.

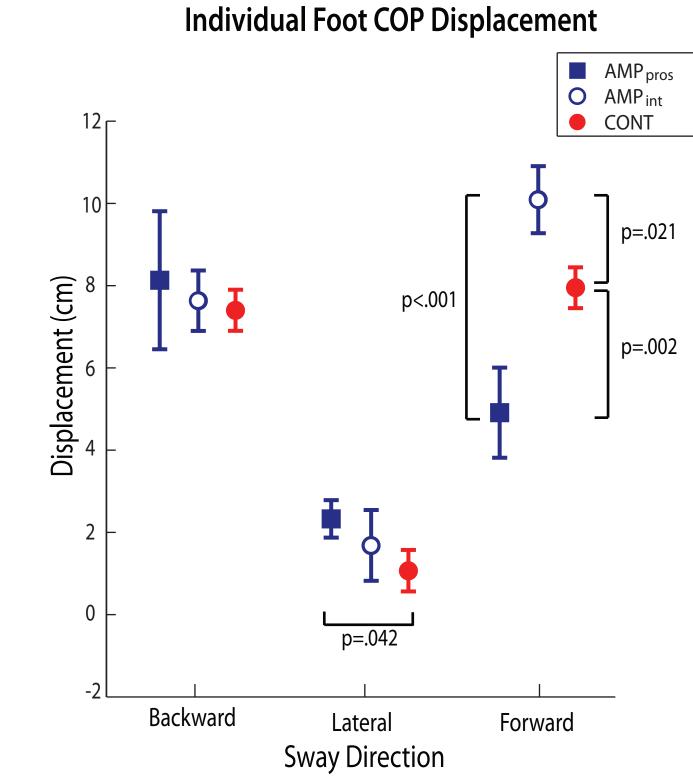
COP responses under each foot differed based on sway direction.

Forward Sway:

- Stability margin and cumulative COP peak displacement (above) did not differ between groups.
- **AMP subjects** had larger COP displacement in the intact leg as compared to both the prosthetic leg (p < 0.001) and **CONT** subjects (p=0.021).

Lateral Sway:

AMP subjects had larger COP displacement in the prosthetic limb when loaded as compared to **CONT subjects** (p=0.042).



Discussion and Conclusions

Intact leg compensates for prosthetic leg deficits in forward sway.

- Ability for COP response in prosthetic foot is limited in forward sway.
- AMP subjects show increased reliance on the intact ankle for balance control in this direction, which is consistent with previous work [7].

Clinical Significance:

- Evaluation of intact leg should not be forgotten.
- Training to improve strength and range of motion of the intact ankle may be needed to enhance balance capabilities.

AMP group maximizes stability margin on prosthetic side.

- Results suggest that AMP subjects are unable to modulate COP displacement when perturbed toward the prosthetic side.
- As a result, maximum COP response leads to a larger stability margin.
- Unclear whether AMP subjects are able to increase balance response to maintain stability margin with more challenging perturbations.

Clinical Significance:

Understanding dynamic balance control in individuals with TTLL can help lead to improved design of prosthetic feet and ankle components.

Future Directions:

- Increase sample size.
- Investigate longer time period for balance response by altering platform parameters to create more complete understanding.
- Analyze EMG and data from additional stance widths already collected.